

# Genetically encoded sensors enable real-time observation of metabolite production

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Engineering cells to produce valuable metabolic products is hindered by the slow and laborious methods available for evaluating product concentration. Consequently, many designs go unevaluated, and the dynamics of product formation over time go unobserved. In this work, we develop a framework for observing product formation in real time without the need for sample preparation or laborious analytical methods. We use genetically encoded biosensors derived from small-molecule responsive transcription factors to provide a fluorescent readout that is proportional to the intracellular concentration of a target metabolite. Combining an appropriate biosensor with cells designed to produce a metabolic product allows us to track product formation by observing fluorescence. With individual cells exhibiting fluorescent intensities proportional to the amount of metabolite they produce, high-throughput methods can be used to rank the quality of genetic variants or production conditions. We observe production of several renewable plastic precursors with fluorescent readouts and demonstrate that higher fluorescence is indeed an indicator of higher product titer. Using fluorescence as a guide, we identify process parameters that produce 3-hydroxypropionate at 4.2 g/L, 23-fold higher than previously reported. We also report, to our knowledge, the first engineered route from glucose to acrylate, a plastic precursor with global sales of \$14 billion. Finally, we monitor the production of glucarate, a replacement for environmentally damaging detergents, and muconate, a renewable precursor to polyethylene terephthalate and nylon with combined markets of \$51 billion, in real time, demonstrating that our method is applicable to a wide range of molecules.

biotechnology | directed evolution | biosensor | metabolic engineering | synthetic biology

**B**iological production of valuable products such as pharmaceuticals or renewable chemicals holds the potential to transform the global economy. However, the rate at which bioengineers are able to engineer new living catalysts is hampered by an exceedingly slow design–build–test cycle. We describe a method to accelerate the design–build–test cycle for metabolic engineering by enabling the observation of product formation within microbes as it occurs.

Biological production of a desired product is accomplished by guiding a low-cost starting material such as glucose through a series of intracellular enzymatic reactions, ultimately yielding a molecule of economic interest. The choice of culture conditions, the creation of enzyme variants, and the tuning of endogenous cellular metabolism create a vast universe of potential designs. Because of the complexity of biology, appropriate genetic designs and culture conditions are not known a priori. Even sophisticated modeling paradigms can result in very large design spaces (1, 2). Evaluating genetic designs or modulating process parameters to achieve a desired outcome is therefore a major bottleneck in the bioengineering design–build–test cycle.

Current methods for evaluating biological production of chemicals rely on slow and laborious techniques such as HPLC and mass spectrometry (MS) (3). Estimates of the throughput of these methods are thousands of samples per day in highly specialized laboratories and hundreds of samples per day in more typical laboratories (3). These rates of evaluation are exceedingly small

compared with typical enzyme library sizes, or the  $1 \times 10^9$  unique genomes that can be built in a day by using multiplexed genome engineering (2). If product formation kinetics are to be observed, many time points over the course of production must be analyzed, further reducing the number of conditions that can be evaluated.

Engineers have begun developing strategies for multiplexed evaluation of metabolite production phenotypes to enable a fully multiplexed design–build–test cycle (1, 4–7). In cases of genetic engineering, such a design cycle would more closely resemble biological evolution, rather than the design approaches inspired by electrical engineering that currently dominate the fields of synthetic biology and metabolic engineering. Strategies for multiplexed design evaluation include selections and screens. Selections, which only allow cells exhibiting a desired phenotype to live, have the potential to evaluate billions of designs simultaneously (3). Selections are limited by their false-positive rate and can be challenging to troubleshoot, especially if high production of the metabolite of interest provides a negative growth phenotype. Genetically encoded biosensors link intracellular metabolite levels to fluorescent protein expression and enable fluorescence-based screens. Combined with fluorescent activated cell sorting (FACS), biosensor-based screens provide evaluation rates of up to  $1 \times 10^8$  designs per day (8, 9).

Genetically encoded biosensors are the most versatile method for coupling cellular fluorescence to the quality of a metabolic engineering design. Genetically encoded biosensors link the expression of a fluorescent protein to the intracellular concentration of a target metabolite through the use of intracellular

## Significance

Advances in biotechnology are enabling engineers to harness natural processes for the production of valuable new chemicals and materials. Cells engineered for chemical production act as renewable factories and redefine what is possible in industries as diverse as manufacturing, pharmaceuticals, and energy. Despite this potential, long and uncertain timelines for bio-based product development hinder progress. Engineering cells for chemical production is challenging because the complexity of biology necessitates many attempted designs before an optimal combination of genetic elements or culture conditions is discovered. In this work, we develop a framework that allows design evaluation to be performed with fluorescence such that microbial chemical production can be monitored in real time without the need for sample preparation or laborious analytical techniques.

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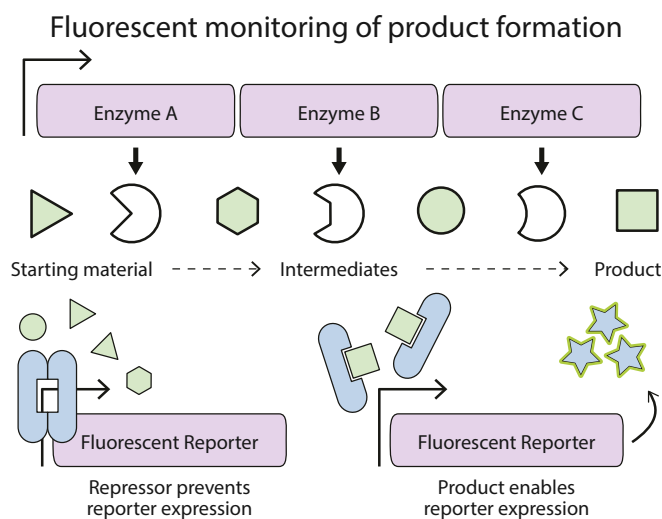
This article contains supporting information online at [www.pnas.org/lookup/suppl/doi:10.1073/pnas.1600375113/-DCSupplemental](http://www.pnas.org/lookup/suppl/doi:10.1073/pnas.1600375113/-DCSupplemental).

switches such as allosterically regulated transcription factors. In addition to the classic small-molecule inducible systems such as *lacI*-IPTG and *tetR*-aTC (10), many new biosensors have been characterized that respond to valuable products as diverse as macrolide antibiotics, flavonoids, and plastic precursors (11).

Our group has previously published detailed characterizations of biosensors that respond to commercially important compounds. Although these studies primarily focused on the biosensors themselves, we did demonstrate that end-point measurements of fluorescence reflect product titers for a single catalytic step (11). However, engineers are typically dealing with metabolic pathways that start with low-cost carbon and energy sources, such as glucose, and proceed through many catalytic steps that are mediated by many gene products, before reaching the target compound. In this work, we monitor product formation through full metabolic pathways and show that the kinetics of product formation can be observed in real time.

Advances in the deployment of biosensors to monitor product formation has been a topic of great interest in recent years and has been well reviewed (12). In many cases, biosensors are used to estimate product titer at a single time point rather than to observe product formation as it takes place. A biosensor designed to respond to a product, while ignoring intermediates, allows the fluorescent readout to act as a real-time proxy for product formation from glucose or other precursors (Fig. 1). This method allows simple observation of performance characteristics such as the rate of product formation or the titer, all without the need for low-throughput analytical pipelines (13).

Observing product formation in real time provides engineers with much greater flexibility in phenotype evaluation than biosensors that are only used to provide a snapshot of the intracellular cell state. For example, the kinetics of production can be used to rank genetic designs when titers exceed biosensor detection limits: Cells with faster production rates can be isolated before sensor saturation. In situations where the pathway



**Fig. 1.** Biosensors enable real-time monitoring of biological chemical production. A metabolic pathway converts a low-cost starting material such as glucose (green triangle) to a desired product (green square) through a series of enzymatic reactions. A biosensor (blue ellipse) regulates the production of a fluorescent reporter by preventing transcription in the absence of the correct inducing molecule. The fluorescent response of the biosensor is proportional to the amount of product produced by the cell because the starting material and intermediates do not activate the biosensor. Each cell reports its rate of chemical production through its fluorescence intensity. Cells with high intensity, and consequently highly productive metabolic pathways, are easily identified.

being optimized is destined for extracellular use—or the end product is toxic and the optimized enzymes will be ported to a new host—the rate of product formation may be more important than final titer. Supplementing various pathway intermediates and evaluating the kinetics of product formation at each step enables engineers to determine pathway bottlenecks and even probe complicated behaviors like product or substrate inhibition.

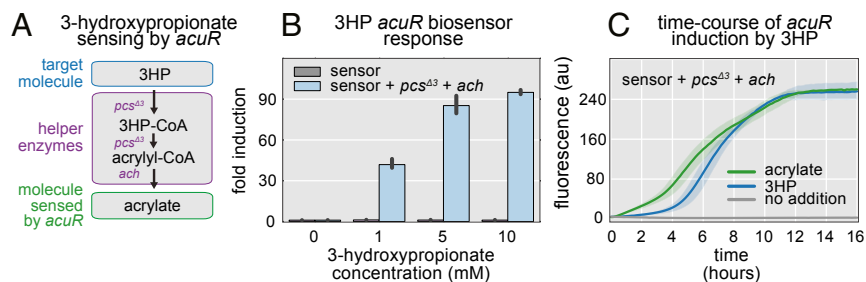
In this work, we develop a strategy for real-time monitoring of metabolic product formation and demonstrate its utility in observing the production of 3-hydroxypropionate (3HP; a renewable plastic precursor) (14), acrylate (the monomer for several common plastics), glucarate (a renewable building block for superabsorbent polymers and a replacement for phosphates in detergents) (15), and muconate (a building block for renewable nylon) (16). We develop two unique biosensors for 3HP and compare their ability to observe 3HP production. We use the real-time observation of 3HP formation to select process parameters that result in a 23-fold increase in 3HP production over previously reported titers. We achieve, to our knowledge, the first direct heterologous route to acrylate by converting 3HP to acrylate in vivo. We go on to demonstrate that this method is applicable to a range of compounds by deploying glucarate and muconate biosensors with their respective heterologous metabolic pathways.

## Results and Discussion

The framework for real-time observation of metabolite production consists of two components: the biosensor and the pathway (Fig. 1). The biosensor is a small-molecule inducible system that produces a fluorescent readout proportional to the amount of product inside of the cell. The pathway consists of all the genes necessary to produce the product molecule from a desired starting point, typically a low-cost feedstock such as glucose or biomass. Rates of product formation vary depending on the amount of intermediate supplied, the number of reactions leading from that intermediate to the final product, and how fast those reactions take place. Final titers depend on these factors as well as the amount of starting material that is shunted into side reactions or used for energy by the cell. We selected pathways for the production of 3HP, glucarate, and muconate from the literature. The acrylate biosynthesis pathway was developed in this study and represents, to our knowledge, the first heterologous route from glucose to acrylate. Previously characterized muconate and glucarate biosensors were combined with their respective production pathways to monitor product formation. Because there are no existing biosensors for 3HP, novel sensors were developed and evaluated for their ability to sense 3HP production in real time.

The first 3HP biosensor was developed from the *Escherichia coli* 2-methylcitrate responsive transcriptional regulator *prpR* (17). Because no 3HP-responsive allosteric transcriptional regulator is known, it was necessary to use a transcriptional regulator that binds to a molecule that 3HP can be converted to intracellularly. The principle of relying on a downstream molecule to affect a response from a nonbinding target compound was pioneered in the Keasling laboratory, when *prpR* and two endogenous enzymes were used to construct a propionate biosensor (18). Here, we use the endogenous enzyme, 2-methylcitrate synthase (*prpC*) and the heterologous multifunctional enzyme propionyl-CoA synthase (*pcs*) from the carbon fixation pathway of *Chloroflexus aurantiacus* (19) to produce 2-methylcitrate from 3HP. Together the system of three genes (*pcs*, *prpC*, and *prpR*) comprise the *prpR*-based 3HP biosensor (*SI Results and Discussion* and Fig. S1).

The second 3HP biosensor was developed from *acuR*, an acrylate responsive transcriptional regulator found in the aquatic bacterium *Rhodobacter sphaeroides* (20). A pathway was constructed that converts 3HP to acrylate (Fig. 2A), allowing the acrylate biosensor to report intracellular 3HP concentration. In this case, a truncated version of the multifunctional enzyme *pcs* is



**Fig. 2.** Development of the 3HP biosensor. (A) Helper enzymes convert 3HP into the *acuR*-binding compound acrylate. (B) The 3HP triggers fluorescence in cells containing the biosensor (blue bars). Higher 3HP results in higher fluorescence. (C) The response of the biosensor to 5 mM 3HP begins immediately and achieves 90% saturation after 8 h (blue line). Induction by 5 mM acrylate is more rapid but achieves the same final fluorescence (green line). Basal induction is low (gray line).

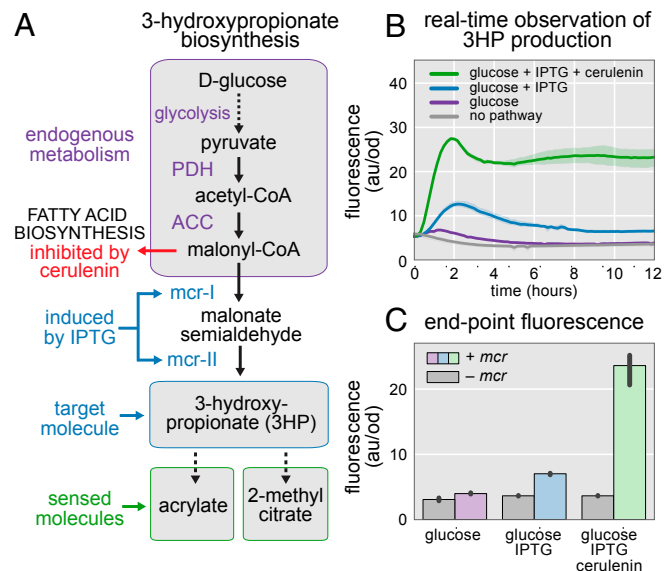
used to convert 3HP into acrylyl-CoA, which is subsequently hydrolyzed to acrylate by the acrylyl-CoA hydrolase (*ach*) from *Acinetobacter baylyi* (21). In *Chloroflexus aurantiacus*, *pcs* catalyzes three subsequent reactions: 3HP to 3HP-CoA to acrylyl-CoA to propionyl-CoA (19). We made use of all three reactions in the *prpR*-based biosensor, but for the *acuR*-based biosensor, accumulation of acrylyl-CoA rather than propionyl-CoA is necessary. Separation of *pcs* into its functional domains has been shown to increase the rates of the individual reactions (22). Because of this finding, we reasoned that we could remove the domain responsible for conversion of acrylyl-CoA to propionyl-CoA while preserving the activity of the other two domains. We refer to the truncated enzyme as *pcs<sup>Δ3</sup>*, and its coexpression with *ach* and *acuR* constitute the *acuR*-based 3HP biosensor (Fig. 2A). Increasing concentrations of 3HP in the medium resulted in increasing levels of fluorescence when *pcs<sup>Δ3</sup>* and *ach* were present, but resulted in no biosensor activation in their absence (Fig. 2B). A 90-fold increase in fluorescence was obtained when the *acuR*-based biosensor was induced with 10 mM 3HP. This result is a much more dramatic activation than that achieved with the *prpR*-based biosensor. The induction kinetics of 3HP and the authentic activator acrylate were compared by monitoring biosensor activation in real time. The 3HP-mediated induction only slightly lagged the time course of acrylate induction (Fig. 2C). Fluorescence remained at background levels for >16 h in the absence of *pcs<sup>Δ3</sup>* and *ach* (Fig. S2).

We coexpressed the 3HP biosensors with the 3HP production pathway to monitor 3HP production in real time (Fig. 3A). The production pathway consists of the endogenous biosynthesis of malonyl-CoA and the bifunctional enzyme malonyl-CoA reductase (*mcr*) from the carbon fixation pathway of *Chloroflexus aurantiacus* (19). *Mcr* shunts malonyl-CoA away from fatty acid biosynthesis by catalyzing the conversion of malonyl-CoA, first into malonate semialdehyde, and then into 3HP, at the expense of two NADPH. This route from glucose to 3HP has been published, with the authors achieving titers of 60 mg/L with expression of *mcr* alone (23). Titters were increased to 180 mg/L with overexpression of the ACC complex and *pntAB*, increasing availability of malonyl-CoA and NADPH, respectively. For our study, we chose to increase the amount of malonyl-CoA available for 3HP production by use of the fatty acid inhibitor cerulenin, rather than through genetic manipulations. Fatty acid biosynthesis is the primary sink for malonyl-CoA and operates at a much higher velocity than heterologously expressed *mcr* (23). Because cerulenin inhibits the activities of *fabB* and *fabF*, increasing its concentration results in lower fatty acid biosynthesis rates and a higher concentration of available malonyl-CoA (24). In each of the 3HP implementations, the biosensor helper enzymes, *pcs* and *pcs<sup>Δ3</sup>/ach*, were constitutively expressed, whereas *mcr* was expressed conditionally with the addition of IPTG.

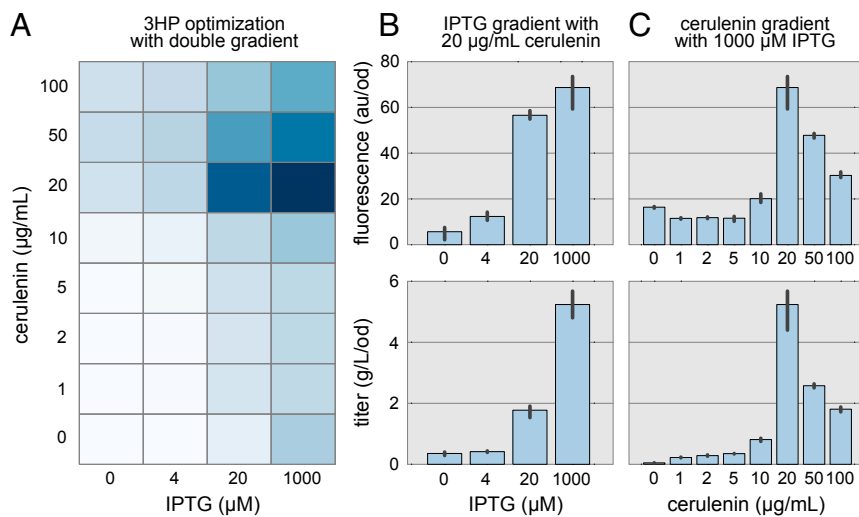
The *acuR*-based 3HP biosensor enables real-time observation of 3HP production (Fig. 3B). In contrast to the *prpR*-based biosensor (SI Results and Discussion and Fig. S3), the *acuR* biosensor is not affected by catabolite repression and facilitates observation of 3HP production in the presence of glucose. *Mcr*

was coexpressed with the *acuR*-based biosensor and fluorescence was observed for 12 h. Cells that were incubated with 50 mM glucose, but without IPTG or cerulenin, produced fluorescence indistinguishable from background levels. Cells incubated with glucose and IPTG showed a significant increase in fluorescence. The most dramatic increase in fluorescence was observed when both IPTG and cerulenin were used. Production of 3HP with glucose, IPTG, and cerulenin resulted in higher rates of GFP expression and end-point fluorescence values than either of the other two conditions. End-point measurements revealed an eightfold increase in fluorescence for *mcr*+ cells vs. *mcr*- cells when incubated with glucose, IPTG, and cerulenin (Fig. 3C). Incubation with glucose and IPTG resulted in a twofold increase in fluorescence compared with cells lacking *mcr*.

The *acuR*-based 3HP biosensor was used to determine optimal concentrations of cerulenin and IPTG for 3HP production (Fig. 4).



**Fig. 3.** Formation of 3HP is observed in real-time. (A) The 3HP is produced from glucose by converting malonyl-CoA into malonate semialdehyde and then on to 3HP. Malonyl-CoA reductase (*mcr*) performs both of these reactions, but competes with fatty acid biosynthesis for malonyl-CoA. (B) The *acuR*-based 3HP biosensor reports the progress of 3HP production in real-time. The addition of 50 mM glucose (purple line) results in a small increase in fluorescence over background (gray line). Addition of IPTG increases the production of *mcr* and the activation of the biosensor (blue line). Providing glucose, IPTG, and cerulenin together results in the most rapid biosensor activation (green line). (C) Fluorescence of the *acuR*-based biosensor after 12 h reveals an approximately fivefold increase in fluorescence in the presence of glucose, IPTG, and cerulenin compared with 3HP production with glucose alone. In the absence of *mcr*, IPTG and cerulenin have no effect on biosensor activation (gray bars). Error bars and confidence bands represent the 95% confidence interval ( $n = 3$ ).



**Fig. 4.** Genetically encoded biosensors were used to identify optimized 3HP production conditions. (A) Eight concentrations of cerulenin and four concentrations of IPTG were combinatorially evaluated in triplicate. Growth-normalized fluorescence of the 96 samples was measured after 24 h (darker shades indicate higher fluorescence). We found that 20 μg/mL cerulenin combined with 1,000 μM IPTG resulted in the greatest biosensor response. (B) The 3HP titer was determined by LC/MS for a range of IPTG concentrations while cerulenin was held constant at 20 μg/mL. (C) The 3HP titer was determined by LC/MS for a range of cerulenin concentrations while IPTG was held constant at 1,000 μM. In both cases fluorescence and titer trended together, verifying the optimal concentrations of IPTG and cerulenin determined by fluorescence alone. Error bars represent the 95% confidence interval ( $n = 3$ ).

Although low levels of cerulenin inhibit fatty acid biosynthesis and make additional malonyl-CoA available for 3HP production, higher concentrations result in poor cell viability and reduced 3HP production. To determine the concentration of cerulenin that achieves the correct balance of these opposing effects, we evaluated eight cerulenin concentrations between 0 and 100 μg/mL. Similarly, high concentrations of IPTG result in high *mcr* gene expression. To determine whether maximal or more nuanced *mcr* expression would achieve optimal 3HP production, we evaluated four levels of IPTG induction. We expected IPTG and cerulenin concentrations to have interacting effects and deemed a combinatorial evaluation of their concentrations necessary. Such an experiment requires 96 samples ( $n = 3$ ) and would be costly to evaluate by using liquid chromatography/mass spectrometry (LC/MS). Instead, we relied on the *acuR*-based 3HP biosensor to determine cerulenin and IPTG concentrations that result in the highest fluorescence response (20 μg/mL cerulenin and 1,000 μM IPTG). We then used MS to determine titers for conditions near this point to verify that the biosensor was indeed identifying optimal production conditions.

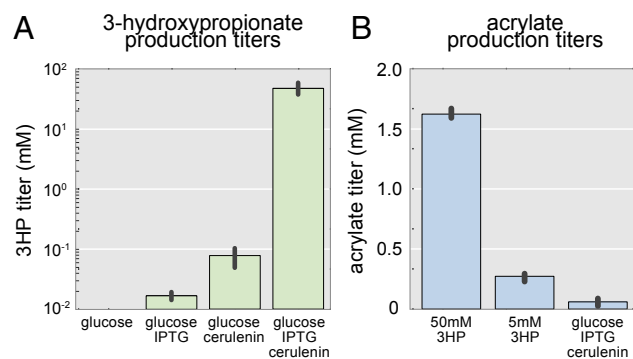
The concentrations of IPTG and cerulenin optimized by use of the 3HP biosensor resulted in a 3HP titer of 4.2 g/L (Fig. 5A). Although higher titers have been attained through a two-step conversion from glycerol, our titers are the highest reported for production of 3HP proceeding through *E. coli* central metabolism (25). These titers were obtained with rich medium in 96-well plates supplemented once with 50 mM glucose at the beginning of fermentation. Production was carried out in BL21 (DE3) transformed with the *mcr* plasmid under the same culture conditions used for the biosensor experiments. Glucose alone produced no detectable 3HP, whereas the addition of 1 mM IPTG resulted in  $1.5 \pm 0.2$  mg/L. The addition of cerulenin resulted in  $7.1 \pm 2.5$  mg/L, whereas addition of both cerulenin and IPTG to the medium resulted in  $4.2 \pm 1.2$  g/L. We were able to produce 23-fold more 3HP than previously reported for the malonyl-CoA route to 3HP. More importantly, the titers achieved here are high enough to warrant further commercial exploration. A major caveat is that these levels of 3HP production rely on the addition of cerulenin, which is not feasible for scale-up due to cost. Our group has previously shown that multiplexed genome engineering combined with static biosensors can obviate the need for cerulenin by finding mutants with increased malonyl-CoA availability (1). Future work will aim to find a similar mutant for 3HP production using the *acuR*-based biosensor developed here.

Coexpression of *pcs*<sup>Δ3</sup> and *ach* enables in vivo production of acrylate (Fig. 5B and Fig. S4). Although biologically derived 3HP

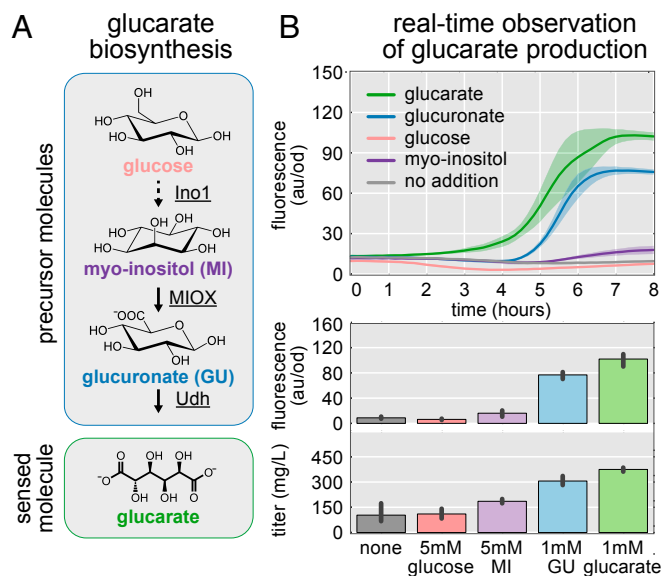
is used to produce several materials, it is most importantly a precursor to biobased acrylate. Currently, 3HP is isolated from cell culture and chemically converted to acrylate (26). In vivo production of acrylate obviates this step by allowing its direct fermentation. We produced  $1.62 \pm 0.05$  and  $0.27 \pm 0.04$  mM acrylate from 50 and 5 mM 3HP, respectively. Addition of the *mcr* plasmid resulted in  $60 \pm 37$  μM acrylate produced from glucose in rich medium. These conversion efficiencies are low for commercial acrylate production, but suitable for tracking 3HP production.

The *acuR*-based 3HP biosensor will be a better choice than the *pppR*-based biosensor for most 3HP production enhancement applications. The lack of catabolite repression and dramatically higher dynamic range are key considerations. Substantial work has been done to remove the catabolite repression from *pppR*, but with little success (27). The fact that *acuR* senses acrylate, which is not naturally present in cells, whereas *pppR* senses 2-methylcitrate, is another important consideration. The background levels of 2-methylcitrate in the cells may account for the elevated basal fluorescence and lower dynamic range of the *pppR* biosensor.

We applied the real-time sensing paradigm to two additional metabolic pathways to demonstrate that real-time observation of product formation is applicable to many biosensor and pathway combinations. The first additional demonstration is the real-time observation of muconate production (SI Results and Discussion



**Fig. 5.** Production titers for 3HP and acrylate. (A) The culture conditions evaluated for biosensor activation were also evaluated for 3HP production. Titers were measured by LC/MS and found to correspond to biosensor activation. A concentration of 4.2 g/L 3HP was produced in rich medium supplemented with glucose, IPTG, and cerulenin. (B) Acrylate production from 3HP and glucose was determined by LC/MS. Error bars represent the 95% confidence interval derived from the SEM ( $n = 3$ ).



**Fig. 6.** Real-time observation of glucarate production. (A) Glucarate is produced from glucose with the expression of three heterologous enzymes of differing activities: Udh has high activity, MIOX has low activity, and Ino1 competes with glycolysis for glucose-6-phosphate. The biosensor monitors the presence of glucarate while ignoring pathway intermediates. (B) Fluorescence is observed over time as pathway intermediates are converted to glucarate. Biosensor activation by glucuronate (blue line) lags behind activation by glucarate (green line). Activation of the biosensor by glucarate or glucuronate occurs more rapidly than activation by either myo-inositol (purple line) or glucose (tan line). This result reflects the relative activities of the enzymes in the glucarate biosynthesis pathway. End-point fluorescence measured after 8 h trends well with the glucarate titers determined by LCMS. Error bars and confidence bands represent the 95% confidence interval ( $n = 3$ ).

and Fig. S5). The second additional demonstration is the real-time observation of glucarate production through the action of three heterologous enzymes.

Glucarate is a US Department of Energy “top value added chemical” to produce from biomass, with applications as a renewable replacement for petrochemicals and as a building block for new ultrahydrophilic polymers (15). Several papers describe construction and optimization of the glucarate biosynthesis pathway (28–30). However, attaining high titers remains challenging because of the low stability and activity of myo-inositol oxygenase, making this pathway a prime target for optimization by directed evolution. The ability to monitor glucarate production in individual cells will enable studies combining flow cytometry and directed mutagenesis.

We combined the previously characterized glucarate biosensor (11) with the glucarate biosynthesis pathway comprising IPTG-inducible myo-inositol-1-phosphate synthase (Ino1; *Saccharomyces cerevisiae*), myo-inositol oxygenase (MIOX; *Mus musculus*), and uronate dehydrogenase (Udh; *Agrobacterium tumefaciens*) (Fig. 6A) (11, 29). We anticipated that the glucarate biosensor would produce a fluorescent response proportional to the amount of glucarate produced within the cell. To evaluate this assumption, we maintained identical production conditions (e.g., genetics, medium composition) but varied the exogenously supplemented precursor molecules, with the hypothesis that compounds further along in the biosynthesis pathway (i.e., separated from glucarate by fewer reactions) would result in more rapid glucarate formation. Addition of glucarate itself resulted in the most rapid accumulation of GFP and ultimately the highest amount of fluorescence (Fig. 6B). As expected, we observed a similar fluorescent response to glucarate in biosensor strains with, and without, the biosynthesis pathway. In contrast, none of the

other exogenously supplied molecules resulted in a fluorescent response in the biosensor strain lacking the glucarate biosynthesis pathway (Fig. S6). This result indicates that glucarate, and not the precursor molecules, trigger the fluorescent response. In the strain containing both the biosensor and the biosynthesis pathway, addition of glucuronate to the medium resulted in a fluorescent response lagging glucarate by  $\sim 90$  min, ultimately achieving an end-point fluorescence that was 80% that of glucarate. This observation is in contrast to the addition of myo-inositol, which resulted in a fluorescence response lagging that of glucuronate by 60 min. Notably, the end-point fluorescence achieved by the addition of myo-inositol is just 20% that of glucuronate addition. Medium supplemented with 50 mM glucose resulted in no fluorescent response within the duration of the experiment (Fig. 5B).

The fluorescent output of the glucarate biosensor reflects the properties of the glucarate biosynthesis pathway. The conversion of glucuronate to glucarate is known to be the fastest heterologous reaction in the biosynthesis of glucarate (29). Correspondingly, we see robust biosensor activation when glucuronate is the starting material. The fluorescent response to myo-inositol addition is slow and corroborates the difficulty of using *M. musculus* MIOX in the catalysis of myo-inositol to glucuronate in *E. coli* (30). The lack of biosensor response to additional glucose may reflect the fact that glucarate biosynthesis is competing with glycolysis for glucose-6-phosphate. It may take substantial Ino1 activity to create meaningful quantities of myo-inositol. Low myo-inositol production would be further compounded by weak MIOX activity, ultimately yielding low glucarate titers and biosensor-mediated fluorescence. Tuning the endogenous metabolism to balance glycolysis with glucarate production, while screening for fluorescence resulting from glucose supplementation, would be a powerful strategy for finding strains that produce high glucarate titers. A similar approach could be taken in searching for a more effective variant of MIOX from a library of targeted or untargeted mutations.

We have found that the fluorescent response of the biosensor is a good proxy for product titer. The fluorescence observed 8 h after addition of the precursor molecules was measured and compared with the glucarate titers achieved under similar conditions. Glucarate production was observed for every condition tested when the cells contained the biosynthesis pathway. No production was observed without the pathway. Glucarate formation was observed in rich LB medium, even without additional substrate added. Addition of 5 mM glucose did not result in a significant increase in glucarate titer within 8 h and is consistent with the observed lack of a fluorescent response. However, addition of myo-inositol resulted in an elevated glucarate titer, as reflected in the fluorescent response. Plotting titer as a function of fluorescence reaffirms that fluorescence is a good predictor of titer across the four culture conditions evaluated here ( $R^2 = 0.96$ ; Fig. S7).

As production titers reach higher values, a biosensor’s upper limit of detection becomes important. When a biosensor becomes saturated, higher concentrations of inducer do not produce a greater fluorescent response. Recent work has revealed detection limits for several biosensors important for biomanufacturing (1, 11). Notably, the glucarate biosensor was shown to have an upper limit of detection  $\sim 15$  mM, whereas the acrylate biosensor was limited by toxicity beyond 5 mM (11). Previous work has shown that the *pppR* biosensor is responsive to propionate at extracellular concentrations beyond 50 mM (18). These detection limits exceed the production achieved here; however, higher detection limits can be attained through biosensor manipulation or incorporation of efflux pumps that reduce intracellular inducer concentration (1).

## Conclusions

Through this work, we have developed a framework for tracking the formation of metabolic products in real time using fluorescent

biosensors. We demonstrated that the fluorescence achieved by a cell is indicative of its productivity—higher fluorescence indicates higher product titers. Fluorescence as a proxy for product titer not only allows for real-time observation of product formation, but also enables cells to report their own individual progress in producing a chemical. Although we have deployed our biosensors for production optimization in 96-well plates, the greatest potential for biosensors is in pathway evaluation via fluorescence-activated cell sorting (FACS). FACS has been used for the optimization of biosynthetic pathways for more than two decades (31). Historically, the metabolic product must have possessed fluorescent properties or been amenable to fluorescent staining (31–33). In contrast, genetically encoded biosensors have enabled FACS to be used for inconspicuous compounds. These studies have shown that biosensor-based FACS can be successful with maximum dynamic ranges as low as 12-fold, indicating that even poorly operating biosensor systems enable multiplexed phenotype evaluation (34). Implementing FACS with our techniques for real-time monitoring of whole pathway biosynthesis will enable greater versatility for phenotype evaluation in metabolic engineering. Furthermore, we have shown that the breadth of metabolic products sensed is not limited by the set of biosensors on hand—one or more downstream

reactions can be used to transform the produced compound into the sensed compound. This strategy is complemented by emerging technologies that enable construction of biosensors for arbitrary compounds (35).

## Methods

Detailed methods can be found in *SI Methods*. A list of plasmids used in this study can be found in [Table S1](#). Production and monitoring of 3HP and acrylate was carried out as follows: DH5 $\alpha$  cells containing the plasmids for the 3HP biosensor were transformed with the plasmid pJKR-MCR and incubated with glucose and different combinations of IPTG and cerulenin. End-point measurements were taken after 12 h. The 3HP and acrylate production titers were determined by LC/MS. Overnight cultures were inoculated 1:100 into 1 mL of LB supplemented with 1 mM IPTG, 20  $\mu$ g/mL cerulenin, and 50 mM glucose in 96-well blocks. Production took place at 37 °C for 16 h. Production of acrylate from glucose was carried out with 50 mM glucose, 1 mM IPTG, and 20  $\mu$ g/mL cerulenin. All production runs were setup in triplicate. Error bars represent the 95% confidence interval derived from the SEM.

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